

ANTERIOR CERVICAL PLATING SYSTEM

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
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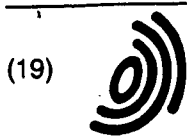
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In one embodiment of the invention, an anterior fixation system (30) includes a plate (31a-31g) defining a plurality of screw holes (34), a number of screws (32) and a number of locking assemblies (33) for fixing the screws (32) to the plate (31a-31g). The system (30) includes two bone screws (32), a fixed angle screw (50) and a variable angle screw (60). Either the fixed or variable angled screws (50, 60) may be implanted with a single plate (31a-31g), and either type of screw (50, 60) may be placed into any of the screw holes (34) along the plate (31a-31g). The several screw holes (34) may be in various patterns (38, 39, 40, 41, 42, 43, 44). The invention further contemplates a locking assembly (33) to lock one or more bone screws (32) within a respective screw hole (34). In one embodiment, the locking assembly (33) includes a washer (90) overlapping one or more screw holes (34), and a locking screw (85). In another embodiment, a locking washer (120) includes cut-outs (128) corresponding to the screw recesses (105), along with a notch (110) and key (129) configuration.

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(54) **ANTERIOR CERVICAL PLATING SYSTEM**

SYSTEM FÜR DIE VORDER-VERPLATTUNG DER HALSWIRBELSÄULE

SYSTEME DE PLAQUE D'OSTEOSYNTHESE CERVICALE ANTERIEURE

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Instrumentation" 1992 , WILLIAMS & WILKINS ,
BALTIMORE,US XP002077159 cited in the
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EP 0 984 728 B1

Description

[0001] The present invention concerns spinal instrumentation systems, most particularly for use in fixation of the cervical spine. More particularly, the invention pertains to a plating system for use in the treatment of various spinal pathologies.

[0002] As with any bony structure, the spine is subject to various pathologies that compromise its load bearing and support capabilities. The spine is subject to degenerative diseases, the effects of tumors and, of course, fractures and dislocations attributable to physical trauma. Throughout the last century, spinal surgeons have tackled the thorny problems associated with addressing and correcting these pathologies using a wide variety of instrumentation and a broad range of surgical techniques. For many years, the use of elongated rigid plates has been helpful in the stabilization and fixation of the lower spine, most particularly the thoracic and lumbar spine. These same plating techniques have found a tougher road towards acceptance by surgeons specializing in treatment of the cervical spine.

[0003] The cervical spine can be approached either anteriorly or posteriorly, depending upon the spinal disorder or pathology to be treated. Many of the well known surgical exposure and fusion techniques of the cervical spine are described in a publication entitled *Spinal Instrumentation*, edited by Drs. Howard An and Jerome Cotler. This text also describes instrumentation that has been developed in recent years for application to the cervical spine, most frequently from an anterior approach.

[0004] The anterior approach to achieving fusion of the cervical spine has become the most popular approach. During the early years of cervical spine fusion, the fusions occurred without internal instrumentation, relying instead upon external corrective measures such as prolonged recumbent traction, the use of halo devices or minerva casts, or other external stabilization. However, with the advent of the elongated plate customized for use in the cervical spine, plating systems have become predominant for this type of spinal surgery.

[0005] It has been found that many plate designs allow for a mono-cortically or bi-cortically intrinsically stable implant. It has also been found that fixation plates can be useful in stabilizing the upper or lower cervical spine in traumatic, degenerative, tumorous or infectious processes. Moreover, these plates provide the additional benefits of allowing simultaneous knurled decompression with immediate stability.

[0006] During the many years of development of cervical plating systems, particularly for the anterior approach, various needs for such a system have been recognized. For instance, the plate must provide strong mechanical fixation that can control movement of each vertebral motion segment in six degrees of freedom. The plate must also be able to withstand axial loading in continuity with each of the three columns of the spine. The

plating system must be able to maintain stress levels below the endurance limits of the material, while at the same time exceeding the strength of the anatomic structures or vertebrae to which the plating system is engaged.

[0007] Another recognized requirements for a plating system is that the thickness of the plate must be small to lower its prominence, particularly in the smaller spaces of the cervical spine. The screws used to connect the plate to the vertebrae must not loosen over time or back out from the plate. Preferably the plate should be designed to contact the vertebrae for greater stability.

[0008] On the other hand, while the plate must satisfy certain mechanical requirements, it must also satisfy certain anatomic and surgical considerations. For example, the cervical plating system must minimize the intrusion into the patient and reduce the trauma to the surrounding soft tissue. In the *Spinal Instrumentation* text, as well as in other documentation in this field, it is stressed that complications associated with any spinal procedure, and most particularly within the tight confines of cervical procedures, the complications can be very devastating, such as injury to the brain stem, spinal cord or vertebral arteries. It has also been found that optimum plating systems permit the placement of more than one screw in each of the instrumented vertebrae.

[0009] Many spinal plating systems have been developed in the last couple of decades that address some of the needs and requirements for cervical fixation systems. However, even with the more refined plating system designs, there still remains a need for a system that has universal applicability to all pathologies that can be faced by a spinal surgeon in treating the spine. For example, it has been demonstrated that different degrees of fixation of a bone screw relative to the plate are more advantageous for treating certain pathologies as opposed to other pathologies.

[0010] More specifically, it is known that bone screws can be supported in a spinal plate in either a rigid or a semi-rigid fashion. In a rigid fashion, the bone screws are not permitted any micro-motion or angular movement relative to the plate. In the case of a semi-rigid fixation, the bone screw can move somewhat relative to the plate during the healing process of the spine. It has been determined that semi-rigid fixation is preferable for the treatment of degenerative diseases of the spine. In cases where a graft is implanted to replace the diseased vertebral body, the presence of a screw capable of some rotation ensures continual loading of the graft. This continual loading avoids stress shielding of the graft, which in turn increases the rate of fusion and incorporation of the graft into the spine.

[0011] Similarly, rigid screw fixation is believed to be preferable in the treatment of tumours or trauma to the spine, particularly in the cervical region. It is believed that tumour and trauma conditions are better treated in this way because the rigid placement of the bone screws preserves the neuro-vascular space and provides for

immediate stabilization. It can certainly be appreciated in the case of a burst fracture or large tumorous destruction of a vertebra that immediate stabilization and preservation of the disc space and neuro space is essential. On the other hand, the semi-rigid fixation is preferable for degenerative diseases because this type of fixation allows for a dynamic construct. In degenerative conditions, a bone graft is universally utilised to maintain either the disc space and/or the vertebral body itself. In most cases, the graft will settle or be at least partially resorbed into the adjacent bone. A dynamic construct, such as that provided by semi-rigid bone screw fixation, will compensate for this phenomenon.

[0012] At present, no plating system is known that allows for the placement of bone screws in either a semi-rigid or a rigid construct with a single plate. While some plates will provide for either one of these screw fixations, no plating system allows the surgeon to use a single plate and to select which of the two types of fixation is desired for the particular spinal pathology and anatomy.

[0013] WO-A-96/29948 describes a bone fixation system that comprises a bone plate with holes along its length and receiving bone screws. The holes are in the form of elongate slots and are configured to receive bone screws in one of two ways. A spherical head bone screw may be used in the slot to provide a variable angle fixing whereas a bone screw with a threaded head can be engaged with threads lining the hole to provide a fixed angle arrangement.

[0014] In order to address the needs left unfulfilled by prior systems, the present invention contemplates a novel system for anterior fixation of the spine utilizing an elongated fixation plate. In one aspect of the invention, the fixation plate is provided with a plurality of holes through which bone screws extend for engagement into a number of vertebrae. In the preferred embodiment, the screw holes include a spherical portion to receive a complementary formed spherical head of the bone screw. The screw holes further include a cylindrical portion integral with the cylindrical portion and opening to the bottom of the plate.

[0015] According to the present invention there is provided a bone fixation system comprising an elongated plate having a top surface and a bottom surface and defining a plurality of holes between said surfaces, at least one of said plurality of holes including a spherical recess portion adjacent said top surface having a first diameter and defining an opening at said bottom surface having a minimum cross-sectional dimension equal to a second diameter which is less than said first diameter; a first bone engaging fastener having a first elongated shank defining bone engaging threads thereon, a first enlarged head and a first intermediate portion between said shank and said head, said first shank having an outer diameter less than said second diameter so said first bone engaging fastener can be inserted through said at least one hole from said top surface of said plate, said first enlarged head defining a partially spherical surface

complementary to said spherical recess of said at least one hole, and said first intermediate portion having a third diameter that is smaller than said second diameter, whereby said first head of said first bone engaging fastener can be pivoted within said recess portion of said at least one hole so that said first bone engaging fastener can assume a plurality of angles relative to said bottom surface of said plate when the first enlarged head engages the recessed portion; and a second bone engaging fastener having a second elongated shank defining bone engaging threads thereon, a second enlarged head and a second intermediate portion between said shank and said head, said second shank having an outer diameter less than said second diameter so said second bone engaging fastener can be inserted through said at least one hole from said top surface of said plate, said second enlarged head defining a partially spherical surface complementary to said spherical recess of said at least one hole, and said second intermediate portion having a portion with a fourth diameter that is approximately equal to said second diameter, whereby said second head of said second bone engaging fastener cannot be pivoted within said recess portion of said at least one hole so that said second bone engaging fastener assumes a fixed orientation relative to said bottom surface of said plate when the second enlarged head engages the recessed portion; characterised in that:

a) the opening is of circular cross-section and defines a cylindrical wall the diameter of which is equal to the second diameter; and

b) the portion of the second bone engaging fastener which has the fourth diameter is cylindrical.

[0016] The flexibility of the present invention anterior fixation plating system is accomplished by the provision of a fixed angle and a variable angle screw that can be supported within the same screw hole in the plate. Each of the screws includes a threaded shank for screwing into a vertebra and a spherical head to seat within the spherical recess. Both screws include an intermediate portion between the spherical head and the threaded shank that is configured to reside within the cylindrical portion of the screw hole when the screw is fixed to the plate. The intermediate portion of the fixed angle screw preferably is cylindrical and has an outer diameter sized for a close fit within the cylindrical portion of the screw hole. In this manner, the fixed angle screw is prevented from rotating or pivoting within the screw hole.

[0017] The variable angle bone screw includes an intermediate portion that is also preferably cylindrical. However, the cylindrical intermediate portion of the variable angle screw has an outer diameter that is significantly smaller than the diameter of the cylindrical portion of the screw hole. This relative difference in diameters between the screw intermediate portion and the screw hole allows the screw to assume a range of angles rel-

ative to the bottom surface of the plate, even when the screw is locked in position in the plate.

[0018] In a further aspect of the invention, a locking assembly is provided for locking the bone screws in the plate, thereby preventing screw back-out. In one embodiment of the invention, the locking assembly includes a washer that resides within a recess in the plate. The recess overlaps at least one screw hole in the plate so that the washer can be seated above the head of the bone screw to hold the screw in place. The locking assembly further includes a threaded set screw that is engaged within a tapped bore concentrically situated within the washer recess. The locking washer is itself configured with a recess so that the head of the locking screw can reside essentially flush within the locking washer.

[0019] In a further embodiment, the locking assembly includes a locking washer having cut-outs formed in its outer surface facing the bone screw head. The cut-outs preferably correspond to the shape of the screw hole so that the washer does not overlap the screw hole in the region of the cut-out. The washer is held to the plate by a set screw to permit rotation of the washer from a first position in which the cut-outs are aligned with the screw holes, to a second position in which the outer surface of the washer overlaps the screw holes to lock the screw heads in position. In a further aspect, the washer includes a number of keys projecting from its underside that are configured to mate within corresponding notches formed in the locking washer recess. The notch and key configuration essentially locks the washer in its position overlapping the screw holes.

[0020] The fixation plate assembly of the present invention further contemplates various screw hole arrangements that permit clamping of multiple screws by a single locking assembly. Other hole arrangements are provided that offer several screw fixation options to the surgeon when instrumenting one or more vertebrae. For instance, a four hole arrangement is set forth in which four screw holes are spaced at 90° intervals around a single locking washer and screw assembly. The surgeon can insert either fixed or variable angle screws into any one or more of the four screw holes depending upon the vertebral anatomy.

[0021] It is one object of the invention to provide a fixation plate assembly that accommodates either fixed or variable angle screw fixation in a single plate. Another object resides in the provision of a locking assembly that can lock one or more bone screws within the plate.

[0022] One benefit achieved by the present invention is that the fixation plate and locking assembly maintain a low profile within the spine. A further benefit is accomplished by the ability to select either a fixed angle or a variable angle screw at any instrumented level and within a single fixation plate.

[0023] Other objects and benefits of the invention will become apparent upon consideration of the following written description of the invention, together with the ac-

companying figures.

DESCRIPTION OF THE FIGURES

[0024]

FIG. 1 is a top perspective view of an anterior plating system according to one embodiment of the present invention.

FIG. 2 is a side elevational view of the plating system shown in FIG. 1.

FIGS. 3(a)-3(g) are top elevational views of a fixation plate in accordance with the present invention provided in different sizes and configuration.

FIG. 4 is a side elevational view of a fixed-angle bone screw according to one aspect of the present invention.

FIG. 5 is a side elevational view of a variable angle bone screw in accordance with another aspect of the present invention.

FIG. 6 is a top elevational view of one embodiment of an elongated plate for use with the anterior plating system according to the present invention.

FIG. 7 is a side cross-sectional view of the plate shown in FIG. 6 taken along line 7-7 as viewed in the direction of the arrows.

FIG. 8 is an end elevational view of the plate shown in FIG. 6.

FIG. 9 is an end cross-sectional view of the plate shown in FIG. 6 taken along line 9-9 as viewed in the direction of the arrows.

FIG. 10 is a partial side view of a portion of the plate shown in FIG. 6, particularly illustrating the four-hole pattern for the bone screw holes.

FIG. 11 is a partial side view of an end of the plate in FIG. 6, particularly showing the end hole pattern of bone screw holes.

FIG. 12 is a transverse cross-sectional view of the end hole pattern of the plate in FIG. 6, particularly taken along line 12-12 in FIG. 11 as viewed in the direction of the arrows.

FIG. 13 is an end transverse cross-sectional view of the end of the plate shown in FIG. 6, particularly taken along line 13-13 in FIG. 11 as viewed in the direction of the arrows.

FIG. 14 is a cross-sectional view of one bone screw opening in the end hole pattern of the plate shown in FIG. 6, particularly taken along line 14-14 in FIG. 8 as viewed in the direction of the arrows.

FIG. 15 is an enlarged side elevational view of a locking screw according to one aspect of the present invention.

FIG. 16 is an enlarged side elevational view of a locking washer in accordance with a further aspect of the present invention.

FIG. 17 is a partial cross-sectional view of an end hole pattern of the plate shown in FIG. 6, with the screw and washer of FIGS. 15 and 16, respectively shown in their operative position.

FIG. 18 is a partial cross-sectional view of a plate according to the present invention with the fixed angle bone screws disposed within bone holes in a plate and engaged within a vertebra.

FIG. 19 is an enlarged end cross-sectional view of the plate according to the present invention with variable angle screws disposed in the plate and engaged in a vertebra.

FIG. 20 is an exploded view of an alternative embodiment of a locking screw assembly for use with an anterior plating system according to a further embodiment of the invention.

FIG. 21 is a top perspective view of the components shown in FIG. 20 in the assembled condition with the locking washer shown in its first position.

FIG. 22 is a top perspective view of the locking screw as depicted in FIG. 20, with the locking washer in its second position.

FIG. 23 is a side elevational view of one embodiment of the locking washer used in the assembly of FIGS. 20-22.

DESCRIPTION OF THE PREFERRED EMBODIMENTS

[0025] For the purposes of promoting an understanding of the principles of the invention, reference will now be made to the embodiment illustrated in the drawings and specific language will be used to describe the same. It will nevertheless be understood that no limitation of the scope of the invention is thereby intended. Any alterations and further modifications in the described device, and any further applications of the principles of the invention as described herein are contemplated as would normally occur to one skilled in the art to which

the invention relates.

[0026] An anterior plating system or fixation assembly 30 is depicted in FIGS. 1 and 2. In accordance with the present invention, the plating system includes an elongated plate 31 and a number of bone screws 32. The bone screws are held to the plate 31 by way of a plurality of locking assemblies 33. The elongated plate 31 is provided with a plurality of screw holes 34 in a variety of arrangements. The plate also can be divided into vertebral level nodes 35 so that the sides of the plate give a serpentine appearance. In particular, the plate 31 includes recesses between each of the nodes 35 to reduce the outer contour and size of the plate. In addition, the reduced width portion between each of the nodes 35 provides an area of reduced material for additional bending of the plate as may be required by the spinal anatomy.

[0027] The plate 31 preferably includes a rounded upper edge 36 that would be in contact with the soft tissue surrounding the spine. The rounded edge 36 reduces the amount of trauma that would be experienced by the surrounding soft tissue. The bottom surface 37 of the plate 31 is preferably configured to contact and engage the vertebral bodies at each of the instrumented levels of the spine. In some embodiments, the bottom surface can be textured to enhance its grip on the vertebral body. [0028] Referring now to FIGS. 3(a)-3(g), several variations of the elongated plate 31 are depicted. It is understood that the anterior plating system according to the present invention can be readily adapted to fix several vertebrae, of course depending upon the length of the plate and the number and arrangement of screw holes 34. The plate depicted in FIGS. 1, 2 and 3(a) includes five vertebral level nodes 35a so that the plate can be engaged to five vertebrae of the spine. For example, the plate 31a of FIG. 3(a) could be used to fix the vertebrae C1-C5. The elongated plates 31b depicted in FIG. 3(b) is sized and configured to span three or four vertebrae, depending upon the instrumented vertebral levels. In this instance, the plate 31b includes four vertebral level nodes 35b, with two nodes at the opposite ends of the plate and two nodes offset from each other in the middle portion of the plate.

[0029] A modification of the plate 31b is depicted in FIG. 3(c). In this case, the plate 31c includes three nodes 35c, with the nodes on the opposite side of the middle portion of the plate being directly aligned at the same vertebral level. The plates of FIGS. 3(d)-3(e), namely plates 31d and 31e, are similar to the plate 31c although their lengths are progressively shorter. The last two plates 31f and 31g, in FIGS. 3(f)-3(g), respectively, provide for instrumentation of two vertebral levels, each having two nodes 35f and 35g, respectively.

[0030] In accordance with the present invention, the elongated plates 31a-31g provide a variety of hole patterns at each of the vertebral level nodes 35a-35g. These hole patterns provide, at a minimum, for at least two bone screws to be engaged into each respective

vertebra. As discussed above, it has been found that the placement of two or more screws in each vertebral body improves the stability of the construct. It is one object of the present invention not only to provide for multiple screw placement in each vertebral body, but also to provide means for locking the screws to the elongated plate to prevent backout or loosening of the bone screws. Consequently, in a further aspect of the invention, various hole patterns are provided that address these objects. One pattern is an end hole pattern 38, as shown at the ends of plate 31 in FIG. 1 and plate 31a in FIG. 3 (a). In this arrangement, two screw holes 34 are laterally disposed at a single node 35a. A single locking assembly is disposed between the two screw holes 34 and is configured to lock bone screws disposed within each respective hole. A similar arrangement is provided by the middle hole pattern 39 in which two screw holes are situated at a single vertebral level. A locking assembly is disposed between the two bone screw holes and is configured to lock bone screws within the respective holes in the same manner as screws are locked in the end hole pattern 38.

[0031] The present invention contemplates a plate carrying four-hole patterns. The four-hole pattern 40 illustrated in FIG. 1 and FIGS. 3(a) and 3(b), provides four bone screw holes 34 in a diamond pattern. A single locking assembly 33 is centrally disposed between all of the bone screw holes so that bone screws within the respective holes are simultaneously locked by the single locking assembly. In the five node plate 31a of FIG. 3 (a), two such four-hole patterns 40 are provided. In the three-node plate 31d of FIG. 3(d), only a single four-hole pattern 40 is required. It can be appreciated that the four-hole pattern 40 provides a great degree of flexibility to the surgeon in determining how many bone screws 32 will be engaged into a single vertebra, and in what arrangement. For example, as shown in FIG. 1, two screws are situated in the laterally opposite screw holes at the vertebral level node 35. Alternatively, bone screws could be placed in the longitudinally opposite screw holes oriented along the length of the plate 31a. Less conventional arrangements contemplate bone screws being placed in immediately adjacent screw holes 34, or placing three bone screws in three of the holes of the four-hole pattern 40. Again, the selection of bone screws and their arrangement can be left to the surgeon and will be based upon the type of correction or fixation required and the anatomy of the particular instrumented vertebra.

[0032] A further arrangement for screw holes 34 is provided by the four-hole cluster 41 depicted in FIGS. 3 (b) and 3(c). In the four-hole cluster 41 in plate 31b, two hole pairs 41a and 41b are provided. Each of the hole pairs includes its own locking assembly to lock the two screws into the screw bores of the respective hole pairs. As shown in FIG. 3(b), the orientation of the particular hole pairs provides one screw hole from each pair generally laterally relative to each other in a single vertebra.

The other of the bone screw holes in each respective pair is longitudinally offset from the central screw holes, being disposed closer to the ends of the plate 31b. In this manner, the two central holes of each of the two holes pairs can be engaged in a single vertebra, while the remaining screw holes of the hole pairs 41a and 41b can be disposed in the superior and inferior adjacent vertebrae. Most preferably, however, each of the screw holes in the four-hole cluster 41 is generally oriented over or slightly offset from a single vertebra. The surgeon then has the option to selected any of the screw holes in the two hole pairs 41a or 41b that is optimally aligned over the vertebra.

[0033] A similar arrangement is found in the plate 31c which includes a four-hole cluster 42. In this case, it can be seen that the four-hole cluster 42 includes two hole pairs 42a and 42b, in a manner similar to the four-hole cluster 41 of FIG. 3(b); however in this case, the hole pairs are arranged closer to each other, principally because the plate 31c is shorter than the plate 31b. In both of the four-hole clusters 40 and 41, the locking assemblies are provided to lock only a pair of bone screw holes rather than all four holes with a single locking assembly.

[0034] The invention further contemplates a three-hole pattern, such as pattern 43 provided in the plate 31f in FIG. 3(f). In this pattern 43, a single locking assembly is used to fix three bone screws within the respective screw holes. A five-hole pattern 44 is provided on plate 31g, as shown in FIG. 3(g). In this five-hole pattern, a single hole is arranged centrally between four outlying holes. Two locking assemblies 33 are provided to lock a pair of the outlying four screw holes together with the central hole. In this configuration, the central hole is held in place by two locking assemblies, while each of the outlying four holes is held in place by a single locking assembly.

[0035] In one important aspect of the present invention, the bone screw 32 can either constitute a fixed angle screw 50, as shown in FIG. 4, or a variable angle screw 60, as shown in FIG 5. Turning first to FIG. 4, the fixed angle screw 50 includes a threaded shank 51. The threaded shank is preferably configured to engage the cancellous bone of a vertebral body. The threaded shank can also include self tapping threads, although the specific illustrated embodiment requires prior drilling and tapping of the vertebral body for insertion of the fixed angle screw 50. The screw 50 includes an intermediate portion 52 that is disposed between the threaded shank 51 and the head 54 of the screw. The threaded shank 51 extends into the intermediate portion 52 by a thread run-out 53, according to standard thread machining practices. As can be seen from FIG. 4, the intermediate portion 52 includes a short segment that does not bear any threads. This short segment has an outer diameter D_1 that will assume significance during consideration of the details of the elongated plate 31 discussed herein.

[0036] The head 54 of the fixed angle screw 50 in-

cludes a tool recess 55 that is configured to receive a driving tool. In one specific embodiment, the tool recess 55 can be a hex recess, or in an alternative embodiment, a TORX® type recess. The head 54 includes a truncated or flattened top surface 56 and a spherical surface 57 between the top surface 56 and the intermediate portion 52. The head 54 includes a height H_1 between the top surface 56 and the intermediate portion 52.

[0037] In one specific embodiment, the intermediate portion 52, and more specifically the segment between the thread run-out 53 and the head 54, has a height of 1.2mm and a diameter of 4.05mm. The height H_1 of the head 54 in this specific embodiment has a dimension of 2.6mm. In this specific embodiment, the dimensions of the head 54 and intermediate portion 52 are calibrated for length of the threaded shank 51 of between 10mm and 20mm. In this specific embodiment, the bone screws are preferably configured for engagement in the cervical spine. In another aspect of the specific embodiment, the root diameter of the threaded shank 51 is tapered over the first four convolutions to the final root diameter, which is about 2.43mm in the specific embodiment.

[0038] Turning to FIG. 5, the details of the variable angle screw 60 can be seen. Like the fixed angle screw 50, the variable angle screw 60 includes a threaded shank 61 and an intermediate portion 62. However, in contrast to the fixed angle screw 50, the intermediate portion 62 has an outer diameter D_2 that is approximately equal to the root diameter of the threaded shank 61. In other words, the diameter D_2 of the intermediate portion 62 of the variable angle screw 60 is less than the diameter D_1 of the intermediate portion 52 of the fixed angle screw 50. Like the fixed angle screw 50, the threads of the shank 61 run out into the intermediate portion 62, leaving the portion 62 with a threaded height of about 0.8mm.

[0039] The variable angle screw 60 also includes a head 64 having a tool recess 65 defined from the truncated top surface 66. The head 64 also includes a spherical surface 67 disposed between the top surface 66 and the intermediate portion 62. The head 64 of the variable angle screw 60 has a height H_2 between the top surface and the intermediate portion that is greater than the height H_1 of the head 54 of the fixed angle screw 50.

[0040] In the specific embodiment of the variable angle screw 60, the head 64 has a height H_2 of about 3.3mm. This greater height is attributable to the smaller diameter D_2 of the intermediate portion 64 relative to the diameter D_1 of the intermediate portion 52 of the fixed angle screw 50. Both the head 54 and the head 64 of the respective screws have a comparable outer diameter, which is 4.88mm in the specific embodiment. In the case of the variable angle screw, the diameter of the spherical surface 67 continues around a greater arc because the intermediate portion 62 has a smaller diameter. In one specific embodiment, the intermediate portion 62 has a diameter D_2 of 2.9mm, compared to the

4.05mm diameter D_1 for the fixed angle screw 50.

[0041] Like the fixed angle screw 50, the variable angle screw 60 can be preferably provided in lengths between 10mm and 20mm, for use at different locations in the spine.

[0042] The engagement of the bone screws 50 and 60 to the elongated plate 31 require further discussion of the details of the plate itself. These details can be discerned with reference to FIGS. 6-14. In FIG. 6, the longer plate 31a is depicted, although it is understood that the various geometric structural aspects of this plate are repeated among each of the plates 31b-31g. As discussed previously, the plate 31a includes undulating edges, with the peaks of the undulation corresponding to the vertebral level nodes 35. The plate material between the nodes is reduced to minimize the bulk of the plate and to provide a thinner plate width in areas that may require additional bending for implantation. In the specific embodiment, a plurality of screw holes 34 is provided throughout the length of the plate and in various patterns. In the illustrated embodiment of FIG. 6, the holes are oriented in end hole patterns 38 at opposite ends of the plate, middle hole pattern 39 centrally located in the plate, and two four-hole patterns 40 disposed between the end hole patterns 38 and the middle hole pattern 39. In each case, the hole patterns require a locking screw assembly 33. Consequently, the plate 31a, along with all the other plate design contemplated by the present invention, includes tapped bore 70 situated within a concentric locking recess 71. (See FIG. 7). As shown in FIGS. 6 and 7, the locking recess 71 intersects or overlaps adjacent bone screw holes 34. In the case of the end hole pattern 38, the locking recess 71 overlaps the two screw holes, while in the case of the four-hole pattern 40, the locking recess 71 overlaps the four holes 34 arranged in a diamond pattern.

[0043] To accommodate the anterior application of this fixation plate assembly 30, the plate is curved in two degrees of freedom. Specifically, the bottom surface 37 of the plate can be curved along a large radius R , as shown in FIG. 7, to accommodate the kyphotic curvature of the cervical spine. In addition, the bottom surface 37 forms a medial/lateral curvature L , as shown in FIG. 9, to correspond to the curvature of the vertebral body. It is understood that the plate 31a can be bent along its longitudinal length between the vertebral level nodes 35, as required to accommodate the particular spinal anatomy and vertebral pathology.

[0044] The screw holes 34 in the plate 31a are defined by a spherical recess 75 (see FIGS. 7 and 9) having a diameter measured about an axis 75a intersecting the elongated plate 31a. (See FIGS. 11 and 12). In a further aspect of the invention, the screw holes 34 include a cylindrical bore 77 communicating between the spherical recess 75 and the bottom surface 37 of the plate 31. The cylindrical bore 77 defines a diameter along the axis 75a. To facilitate insertion of drill guides, drills and the bone screws 32, each screw hole 34 includes a flared

recess 79. The flared recess is preferably formed as a tapered counter-sink along an axis 79a (see FIGS. 11 and 13). This flared recess 79 overlaps the locking recess 71 of the locking assembly 33 at a recess overlap 80, shown best in FIGS. 7, 9 and 13.

[0045] In one specific embodiment, the spherical recess 75 is defined at a diameter of 5.0mm, which is slightly larger than the diameter of the heads 54, 64 of the bone screws 50, 60. The cylindrical portion of the screw holes 34 is defined at a diameter of 4.1mm, in the specific embodiment, which is again slightly larger than the diameter D_1 of the intermediate portion 52 of the fixed angle screw 50. It should be understood, of course, that the diameter of the cylindrical bore 77 is significantly larger than the diameter D_2 of the intermediate portion 62 of the variable angle screw 60.

[0046] Again in the specific embodiment, the axis 75a of both the spherical recess 25 and the cylindrical bore 77 is oriented generally normal to the bottom surface 37 of the plate 31a, when viewed in the direction of the longitudinal axis of the plate. In other words, the axis 75 is normal to the plate in the direction of the medial/lateral curvature L of the plate. On the other hand, the orientation of the screw holes 34 can vary between the vertebral level nodes 35, and most particularly when considering the end hole patterns 38. In this specific embodiment, the flared recess 79, and specifically its axis 79a, can be colinear with the axis 75a of the recess 75, for the hole patterns in the interior of the elongated plate 31a. For example, as shown in FIG. 6, the flared recess 79 can be approximately concentric with the screw holes 34 for the middle hole pattern 39. On the other hand, the flared recess 79, and specifically the axis 79a, at the end hole patterns 38, are offset at an angle A, as depicted in FIG. 14. In particular, the axis 75a of the spherical recess is offset at an angle A of about 12 degrees relative to a perpendicular from the bottom surface 37 of the plate 31a. In this manner, the bone screws will be directed outwardly toward the end of the plate upon insertion into the screw holes 34.

[0047] The details of the locking assembly 33 can be gleaned from consideration of FIGS. 15-17. In this specific embodiment, the locking assembly 33 includes a locking screw 85 having machine threads 86. In one specific embodiment, the locking screw 85 terminates in a sharp point 86a to permit penetration of the vertebral body. The head 87 of the locking screw 85 includes a lower conical surface 88 and a tool recess 89 defined therein for receiving a driving tool.

[0048] The locking assembly 33 also includes a washer 90 having an outer surface 91. In the specific preferred embodiment, the outer surface 91 is defined by a curved convex surface 92. The washer 90 also includes a screw bore 93 extending therethrough in communication with a tapered bore 94. The tapered bore 94 has a complementary mating configuration relative to the conical surface 88 of the head 87 of locking screw 85. The mating conical features between the locking

screw and washer provides a self-centering capability for the washer as the locking screw is tightened onto the plate. The screw bore 93 is sized to receive the machine threads 86 therethrough for engagement with the tapped bore 70 of the plate 31a, as shown in FIG. 17.

As illustrated in FIG. 17, the outer surface 91 of the washer 90 intersects the recess overlap 80 between the flared recess 79 and the respective spherical recess 75 of the adjacent screw holes 34. In a specific embodiment, the locking recess 71 has a diameter of 6mm to accept the washer 90 having an outer diameter of 5.3mm. Again in this specific embodiment, the curved convex surface 92 of the washer 90 is curved at a radius of about 2.5mm so that the lowermost portion of the washer has a smaller diameter of about 4.3mm.

[0049] Referring now to FIGS. 18 and 19, the use of the fixation plate assembly 30 is illustrated. In FIG. 18, a pair of fixed angle screws 50 are disposed within respective bores 34 so that the threaded shanks 51 project beyond the lower surface 37 of the plate 31 and into the vertebral body V. The intermediate portion 52 of the fixed angle screw 50 extends through the cylindrical bore 77 of the screw holes 34. The spherical surface 57 of the head 54 of the screw contacts the spherical recess 75 of the screw hole 34 as the fixed angle screw 50 is threaded into the vertebral body V. Once the screw 50 is completely seated within the spherical recess 75, the intermediate portion 52 provides a snug relationship relative to the cylindrical bore 77 so that the fixed angle screw 50 is not able to pivot or translate relative to the plate 31.

[0050] In order to ensure secure fixation of the screw 50 within plate 31, the locking assembly 33 is tightened onto the heads 54 of the two bone screws 50. In particular, the locking screw 85 is threaded into the tapped bore 70 to draw the washer 90 into contact with the screw heads. The convex surface 92 seats against the spherical surface 57 of the bone screw heads 54 to firmly seat the screw heads within the plate spherical recess 75. Preferably, the locking washer 90 will advance sufficiently far into the locking recess 71 to rest substantially flush with the top surfaces 56 of the bone screws 50. In the locked position, the washer 90 does not bottom out within the locking recess 71.

[0051] In a further aspect of the invention, the locking assembly 33 is loosely fixed on the plate 31 so that the surgeon need not fiddle with the locking assembly when the plate is engaged to a vertebra. In particular, the locking screw 85 is pre-threaded through the locking washer 90 and into the tapped bore 70 until about three or fewer threads of the locking screw project below the bottom surface 37 of the plate. The locking screw 85 is then staked at the thread nearest the plate so that the screw cannot be removed or backed out through the tapped bore 70. Of course, the locking screw 85 can be advanced further through the bore 70 when it is necessary to enable the locking assembly 33. As previously mentioned, the sharp point 86a of the locking screw 85 is

preferably configured to penetrate the cortical bone. With the locking screw staked to the plate, the sharp point 86a will penetrate the vertebra V when the plate 31 is initially positioned on the bone. In this instance, the locking screw 85 helps locate and temporarily stabilize the plate on the vertebra V as the bone screws 50 are implanted into the bone. This temporary location feature provided by the locking screw 85 can also be used when a drill guide is used to drill and tap the vertebra to receive the bone screws 50.

[0052] The locking assembly 33 is configured so that the washer 90 can be moved clear of the screw holes 34 when the locking screw 85 is staked to the plate 31. Thus, even with the locking assembly 33 in its loosened position, the bone screws 50, 60 can still be inserted into the screw holes 34, preferably by pulling the washer 90 away from the plate 31.

[0053] The use of the variable angle bone screw 60 is depicted in FIG. 19. The locking assembly 33 functions as described above to lock the heads 64 of the variable angle screws 60 within the plate 31. Specifically, the convex surface 92 of the washer 90 contacts and applies pressure to the spherical surfaces 67 of the respective bone screws 60. However, with the variable angle screws 60, the intermediate portion 62 does not fit snugly within the cylindrical bore 77 of the screw holes 34. Thus, even with the head 64 of each screw 60 residing solidly within the spherical recess 75, the bone screw 60 can still be angulated relative to the plate and to the axis of the spherical recess 75 and cylindrical bore 77. It is understood that the degree of angulation is restricted by the difference in diameters between the cylindrical bore 77 and the intermediate portion 62 of the variable angle screw 60. In one preferred embodiment, the relative diameters permit angulation of up to 20° from the axis 75a of the recess 75 and bore 77.

[0054] During implantation, the variable angle capability of the screw 60 allows the surgeon to place the bone screw within the vertebra at any angle within the defined angulation limits (20° in one specific embodiment). Thus, the variable angle screw 60 provides greater flexibility than does the fixed angle screw 50 for orienting the bone screw relative to the anatomy of the vertebra. Moreover, this variable angle capability allows a limited degree of micro-motion between the screw and the plate when the fixation assembly 30 is implanted within a patient. In other words, as the spine is loaded and as load is transmitted through the screws and plate, the plate and vertebra may translate relative to each other. The variable angle screw 60 accommodates this relative movement by pivoting within the spherical recess 75. On the other hand, the fixed angle screw 50 prevents this relative movement. The choice between using a fixed or a variable angle screw can be left to the surgeon depending upon the pathology being treated. The fixation plate assembly 30 according to the present invention allows this choice to be made at any point during the surgical procedure.

[0055] A further embodiment of the present invention is depicted in FIGS. 20-23. In this embodiment, an alternative locking mechanism is provided. A plate assembly 100 includes an elongated plate 101 receiving bone screws 102. A locking assembly 103 is provided to lock the bone screw within the plate. The plate 101 defines a spherical recess 105 to receive the spherical head 115 of the bone screw. The threaded shank 114 of the bone screw projects through the recess. It is understood that the bone screw 102 and spherical recess 105 can be similar to the like components described above.

[0056] In accordance with this embodiment, the plate further includes a tapped bore and concentric locking recess 107 disposed adjacent the spherical recess 105 for the bone screw. The spherical and locking recess contact at a locking overlap 108. A notch 110 extends transversely across the locking recess 107 in this embodiment.

[0057] The locking assembly 103 includes a locking washer 120 and locking screw 121. Like the prior locking screw, the screw 121 includes machine threads 122 and an enlarged head 123. The head sits within a recess 124 in the washer 120, with the machine threads 122 projecting through a bore 125. The machine threads 122 are configured to engage the tapped bore 106 of the plate 101. The locking screw 121 can be staked onto the plate 101 as discussed with respect to the prior embodiment.

[0058] The locking washer 120, while functioning similar to the washer of the prior embodiment, offers a different construction than the previous washer. Like the washer 90, the locking washer 120 includes an outer circumferential surface 127 that is preferably convex to mate with a spherical head of the bone screw 102. However, in one modification, the washer 120 includes cut-outs 128 in the circumferential surface 127. The cut-outs 128 are arranged to coincide with the screw recesses 105 when the locking washer is in a first position, as illustrated in FIG. 21. This structure of the washer 120 allows the washer to remain clear of the recess 105 for unimpeded insertion of the bone screw 102.

[0059] In certain embodiments, the washer 120 is provided with two such cut-outs at diametrically opposite positions on the washer. Most preferably, the cut-outs 128 aligned with the relative orientation of screw holes 105 in the plate 101. For example, a washer 120 adapted for a three hole pattern 43, as depicted in FIG. 3(f), would have three cut-outs 128 at 120° intervals. Similarly, a locking washer 120 modified for use with the four hole pattern 40 of FIG 3(a) would have four cut-outs 128 spaced 90° apart on the circumferential surface 127 of the washer.

[0060] Once the bone screws have been implanted through the appropriate screw recesses 105, the locking washer 120 can be rotated into its locking position shown in FIG. 22. In this position, the cut-outs 128 are rotated away from the screw recesses 105 so that the washer, and more particularly the outer circumferential

surface 127, overlaps the screw recess 105. In a further modification from the prior washer, the washer 120 includes a number of keys 129 on the underside of the washer. The keys are configured to sit within a corresponding notch 110 in the plate 101 when the locking washer is in the locking position shown in FIG. 22. Once the bone screws have been implanted and the locking washer 120 has been rotated into its locking position, the keys 129 fall into the notches 110 to fix the position of the washer while the locking screw 121 is tightened.

[0061] While the invention has been illustrated and described in detail in the drawings and foregoing description, the same is to be considered as illustrative and not restrictive in character, it being understood that only the preferred embodiments have been shown and described and that all changes and modifications that come within the scope of the invention as defined in the appended claims are desired to be protected.

Claims

1. A bone fixation system comprising:

an elongated plate (31) having a top surface and a bottom surface (37) and defining a plurality of holes (34) between said surfaces, at least one of said plurality of holes including a spherical recess portion (75) adjacent said top surface having a first diameter and defining an opening (77) at said bottom surface (37) having a minimum cross-sectional dimension equal to a second diameter which is less than said first diameter;

a first bone engaging fastener (60) having a first elongated shank (61) defining bone engaging threads thereon, a first enlarged head (64) and a first intermediate portion (62) between said shank and said head, said first shank having an outer diameter less than said second diameter so said first bone engaging fastener (60) can be inserted through said at least one hole (34) from said top surface of said plate (31), said first enlarged head (64) defining a partially spherical surface (67) complementary to said spherical recess (75) of said at least one hole, and said first intermediate portion (62) having a third diameter that is smaller than said second diameter, whereby said first head (64) of said first bone engaging fastener can be pivoted within said recess portion (75) of said at least one hole (34) so that said first bone engaging fastener (60) can assume a plurality of angles relative to said bottom surface (37) of said plate when the first enlarged head (64) engages the recessed portion (75); and

a second bone engaging fastener (50) having a second elongated shank (51) defining bone

engaging threads thereon, a second enlarged head (54) and a second intermediate portion (52) between said shank and said head, said second shank (51) having an outer diameter less than said second diameter so said second bone engaging fastener (50) can be inserted through said at least one hole (34) from said top surface of said plate (31), said second enlarged head (54) defining a partially spherical surface (57) complementary to said spherical recess (75) of said at least one hole (34), and said second intermediate portion (52) having a portion with a fourth diameter that is approximately equal to said second diameter, whereby said second head (54) of said second bone engaging fastener (50) cannot be pivoted within said recess portion (75) of said at least one hole (34) so that said second bone engaging fastener assumes a fixed orientation relative to said bottom surface (37) of said plate (31) when the second enlarged head engages the recessed portion; characterised in that:

a) the opening (77) is of circular cross-section and defines a cylindrical wall the diameter of which is equal to the second diameter; and

b) the portion of the second bone engaging fastener (50) which has the fourth diameter is cylindrical.

2. The bone fixation system of claim 1, further comprising a locking screw assembly (33) for locking said heads of said bone engaging fasteners (50; 60) within said spherical recess portion (75) of said plate (31).

3. The bone fixation system of claim 2, wherein said locking screw assembly (33) includes:

a fastener bore (70) defined in said plate (31) adjacent said at least one hole (34);

a washer (90) defining a central aperture (93) and a recess (94) communicating with said aperture, said washer further having an outer circumferential surface (91) configured to contact said head (54; 64) of said bone engaging fastener (50; 60) extending through said at least one hole (34); and

a locking fastener (85) having a head (87) configured to be recessed within said recess (94) of said washer (90) and an elongated shank extending through said central aperture (93) and configured to engage said fastener bore (70) of said plate (31).

4. The bone fixation system of claim 3, wherein said

outer circumferential surface (91) of said washer (90) has a concave curvature substantially corresponding to said partially spherical surface (57; 67) of said head of said bone engaging fastener (50; 60).

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5. The bone fixation system of claim 3 or 4, wherein said plate (31) further defines a locking recess (71) in said top surface concentric with said fastener bore (70) and said at least one hole (34) includes a flared recess (79) overlapping said locking recess (71). 10
6. The bone fixation system of claims 3, 4 or 5, wherein the washer (90; 120) has a bottom surface configured to contact said head of said bone engaging fastener when said bone engaging fastener is extended through said at least one hole, said washer (120) further defining a circumferential surface having a first portion (127) overlapping said at least one hole (34) when said washer is in a first position relative to said at least one hole and having a second portion (128) that does not overlap said at least one hole when said washer is rotated from said first position to a second position, whereby said bone engaging fastener can be inserted through said at least one hole with said washer engaged to said plate when said washer is in said second position. 15 20 25
7. The bone fixation system of any of claims 3, 4, 5 or 6, further comprising a notch (110) defined in said plate (31) adjacent said fastener bore, said washer including a key (129) adjacent said central aperture configured to seat within said notch in said plate to prevent rotation of said washer relative to said plate. 30 35
8. The bone fixation system of any preceding claim, wherein the elongated plate defines a plurality of vertebral nodes (35) along the length of the plate. 40
9. A bone fixation system according to claim 8, wherein at least two holes (34) are provided at a corresponding one node (35).
10. The bone fixation system according to any preceding claim, wherein said elongated plate (31) has a rounded edge (36) extending between said top and bottom surfaces. 45
11. The bone fixation system according to any preceding claim, wherein the fastener heads include a truncated top surface (56). 50
12. The bone fixation system according to any preceding claim, wherein the bone engaging threads of said first and second bone engaging fasteners (50; 60) are self tapping. 55

13. The bone fixation system of any preceding claim, wherein said third diameter is about 2.90 millimetres and said fourth diameter is about 4.05 millimetres.

Patentansprüche

1. Knochenfixierungssystem, das Folgendes umfasst:

eine längliche Platte (31) mit einer Oberseite und einer Unterseite (37) und einer Mehrzahl von Löchern (34) zwischen den genannten Seiten, wobei wenigstens eines aus der genannten Mehrzahl von Löchern einen sphärischen ausgesparten Abschnitt (75) neben der genannten Oberseite hat, der einen ersten Durchmesser hat und eine Öffnung (77) an der genannten Unterseite (37) definiert, die eine Mindestquerschnittsgröße hat, die einem zweiten Durchmesser entspricht, der kleiner als der genannte erste Durchmesser ist;

ein erstes in den Knochen eingreifendes Befestigungsmittel (60) mit einem ersten länglichen Schaft (61) mit einem Knocheneingriffsgewinde daran, einem ersten vergrößerten Kopf (64) und einem ersten Zwischenabschnitt (62) zwischen dem genannten Schaft und dem genannten Kopf, wobei der genannte erste Schaft einen Außendurchmesser hat, der kleiner als der genannte zweite Durchmesser ist, so dass das genannte erste in den Knochen eingreifende Befestigungsmittel (60) durch das genannte wenigstens eine Loch (34) von der genannten Oberseite der genannten Platte (31) eingesetzt werden kann, wobei der genannte erste vergrößerte Kopf (64) eine teilweise sphärische Oberfläche (67) hat, die komplementär zu der genannten sphärischen Aussparung (75) des genannten wenigstens einen Lochs ist, und wobei der genannte erste Zwischenabschnitt (62) einen dritten Durchmesser hat, der kleiner als der genannte zweite Durchmesser ist, wobei der genannte erste Kopf (64) des genannten ersten in den Knochen eingreifenden Befestigungsmittels innerhalb des genannten ausgesparten Abschnitts (75) des genannten wenigstens einen Lochs (34) schwenkbar ist, so dass das genannte erste in den Knochen eingreifende Befestigungsmittel (60) eine Mehrzahl von Winkeln relativ zu der genannten Unterseite (37) der genannten Platte bilden kann, wenn der erste vergrößerte Kopf (64) in den ausgesparten Abschnitt (75) eingreift; und

ein zweites in den Knochen eingreifendes Befestigungsmittel (50) mit einem zweiten länglichen Schaft (51) mit einem Knocheneingriffsgewinde daran, einem zweiten vergrößerten

Kopf (54) und einem zweiten Zwischenabschnitt (52) zwischen dem genannten Schaft und dem genannten Kopf, wobei der genannte zweite Schaft (51) einen Außendurchmesser hat, der kleiner als der genannte zweite Durchmesser ist, so dass das genannte zweite in den Knochen eingreifende Befestigungsmittel (50) von der genannten Oberseite der genannten Platte (31) durch das genannte wenigstens eine Loch (34) eingesetzt werden kann, wobei der genannte zweite vergrößerte Kopf (54) eine teilsphärische Oberfläche (57) hat, die komplementär zu der genannten sphärischen Aussparung (75) des genannten wenigstens einen Lochs (34) ist, und wobei der genannte zweite Zwischenabschnitt (52) einen Abschnitt mit einem vierten Durchmesser hat, der etwa dem genannten zweiten Durchmesser entspricht, wobei der genannte zweite Kopf (54) des genannten zweiten in den Knochen eingreifenden Befestigungsmittels (50) nicht innerhalb des genannten ausgesparten Abschnitts (75) des genannten wenigstens einen Lochs (34) schwenkbar ist, so dass das genannte zweite in den Knochen eingreifende Befestigungsmittel eine feste Ausrichtung relativ zu der genannten Unterseite (37) der genannten Platte (31) annimmt, wenn der zweite vergrößerte Kopf in den ausgesparten Abschnitt eingreift; **dadurch gekennzeichnet, dass:**

- a) die Öffnung (77) einen kreisförmigen Querschnitt hat und eine zylindrische Wand definiert, deren Durchmesser dem zweiten Durchmesser entspricht; und
- b) der Abschnitt des zweiten in den Knochen eingreifenden Befestigungsmittels (50) mit dem vierten Durchmesser zylindrisch ist.

2. Knochenfixierungssystem nach Anspruch 1, ferner umfassend eine Sicherungsschraubenbaugruppe (33) zum Sichern der genannten Köpfe der genannten in den Knochen eingreifenden Befestigungsmittel (50; 60) in dem genannten sphärischen ausgesparten Abschnitt (75) der genannten Platte (31).
3. Knochenfixierungssystem nach Anspruch 2, wobei die genannte Sicherungsschraubenbaugruppe (33) Folgendes umfasst:

eine Befestigungsmittelbohrung (70) die in der genannten Platte (31) neben dem genannten wenigstens einen Loch (34) definiert ist;
eine Unterlegscheibe (90) mit einer mittleren Apertur (93) und einer Aussparung (94), die mit der genannten Apertur verbunden ist, wobei die genannte Unterlegscheibe ferner eine äußere

Umfangsfläche (91) hat, die so konfiguriert ist, dass sie mit dem genannten Kopf (54; 64) des genannten in den Knochen eingreifenden Befestigungsmittels (50; 60) in Kontakt ist, die durch das genannte wenigstens eine Loch (34) verläuft; und

ein sicherrides Befestigungsmittel (85) mit einem Kopf (87), der so konfiguriert ist, dass er innerhalb der genannten Aussparung (94) der genannten Unterlegscheibe (90) versenkt wird, und einem länglichen Schaft, der durch die genannte mittlere Apertur (93) verläuft und so konfiguriert ist, dass er in die genannte Befestigungsmittelbohrung (70) der genannten Platte (31) eingreift.

4. Knochenfixierungssystem nach Anspruch 3, bei dem die genannte äußere Umfangsfläche (91) der genannten Unterlegscheibe (90) eine konkave Krümmung hat, die im Wesentlichen der genannten teilsphärischen Fläche (57; 67) des genannten Kopfes des genannten in den Knochen eingreifenden Befestigungsmittels (50; 60) entspricht.
5. Knochenfixierungssystem nach Anspruch 3 oder 4, wobei die genannte Platte (31) ferner eine Sicherungsaussparung (71) in der genannten Oberseite aufweist, die mit der genannten Befestigungsmittelbohrung (70) konzentrisch ist, und das genannte wenigstens eine Loch (34) eine aufgeweitete Aussparung (79) beinhaltet, die die genannte Sicherungsaussparung (71) überlappt.
6. Knochenfixierungssystem nach Anspruch 3; 4 oder 5, wobei die Unterlegscheibe (90; 120) eine Unterseite hat, die so konfiguriert ist, dass sie den genannten Kopf des genannten in den Knochen eingreifenden Befestigungsmittels kontaktiert, wenn das genannte in den Knochen eingreifende Befestigungsmittel durch das genannte wenigstens eine Loch verläuft, wobei die genannte Unterlegscheibe (120) ferner eine Umfangsfläche mit einem ersten Abschnitt (127) definiert, der das genannte wenigstens eine Loch (34) überlappt, wenn sich die genannte Unterlegscheibe in einer ersten Position relativ zu dem genannten wenigstens einen Loch befindet, und mit einem zweiten Abschnitt (128), der das genannte wenigstens eine Loch nicht überlappt, wenn die genannte Unterlegscheibe von der genannten ersten Position in eine zweite Position gedreht wird, so dass das genannte in den Knochen eingreifende Befestigungsmittel durch das genannte wenigstens eine Loch eingesetzt werden kann, wobei sich die genannte Unterlegscheibe im Eingriff mit der genannten Platte befindet, wenn die genannte Unterlegscheibe in der genannten zweiten Position ist.

7. Knochenfixierungssystem nach einem der Ansprüche 3, 4, 5 oder 6, ferner umfassend eine Kerbe (110) in der genannten Platte (31) neben der genannten Befestigungsmittelbohrung, wobei die genannte Unterlegscheibe eine Passfeder (129) neben der genannten mittleren Apertur hat, die so konfiguriert ist, dass sie in der genannten Kerbe in der genannten Platte sitzt, um eine Drehung der genannten Unterlegscheibe relativ zu der genannten Platte zu verhindern. 5 10
8. Knochenfixierungssystem nach einem der vorherigen Ansprüche, wobei die längliche Platte eine Mehrzahl von Wirbelknoten (35) entlang der Länge der Platte aufweist. 15
9. Knochenfixierungssystem nach Anspruch 8, wobei wenigstens zwei Löcher (34) an jeweils einem entsprechenden Knoten (35) vorgesehen sind. 20
10. Knochenfixierungssystem nach einem der vorherigen Ansprüche, wobei die genannte längliche Platte (31) eine abgerundete Kante (36) hat, die zwischen der genannten Ober- und Unterseite verläuft. 25
11. Knochenfixierungssystem nach einem der vorherigen Ansprüche, wobei die Befestigungsmittelköpfe eine kegelstumpfförmige Oberseite (56) haben. 30
12. Knochenfixierungssystem nach einem der vorherigen Ansprüche, wobei die Knocheneingriffsgewinde des genannten ersten und zweiten in den Knochen eingreifenden Befestigungsmittels (50; 60) selbstschneidend sind. 35
13. Knochenfixierungssystem nach einem der vorherigen Ansprüche, wobei der genannte dritte Durchmesser etwa 2,90 Millimeter und der genannte vierte Durchmesser etwa 4,05 Millimeter beträgt. 40

Revendications

1. Système d'ostéosynthèse comprenant: 45

une plaque allongée (31) présentant une surface supérieure et une surface inférieure (37) et définissant une pluralité de trous (34) entre lesdites surfaces, au moins un de ladite pluralité de trous comprenant une partie renforcée sphérique (75) à proximité de ladite surface supérieure ayant un premier diamètre et définissant une ouverture (77) au niveau de ladite surface inférieure (37) dont la dimension de section minimale est égale à un deuxième diamètre qui est inférieur audit premier diamètre; 50 55

un premier élément de fixation d'engagement

avec un os (60) comportant une première tige allongée (61) définissant sur elle des filetages d'engagement avec un os, une première tête élargie (64) et une première partie intermédiaire (62) entre ladite tige et ladite tête, ladite première tige ayant un diamètre extérieur inférieur audit deuxième diamètre de sorte que ledit premier élément de fixation d'engagement avec un os (60) peut être inséré à travers ledit au moins un trou (34) depuis ladite surface supérieure de ladite plaque (31), ladite première tête élargie (64) définissant une surface partiellement sphérique (67) complémentaire audit renforcement sphérique (75) dudit au moins un trou, et ladite première partie intermédiaire (62) ayant un troisième diamètre qui est inférieur audit deuxième diamètre, moyennant quoi ladite première tête (64) dudit premier élément de fixation d'engagement avec un os peut être pivotée à l'intérieur de ladite partie renforcée (75) dudit au moins un trou (34) de sorte que ledit premier élément de fixation d'engagement avec un os (60) peut prendre une pluralité de positions angulaires par rapport à ladite surface inférieure (37) de ladite plaque lorsque la première tête élargie (64) est insérée dans la partie renforcée (75); et

un deuxième élément de fixation d'engagement avec un os (50) comportant une deuxième tige allongée (51) définissant sur elle des filetages d'engagement avec un os, une deuxième tête élargie (54) et une deuxième partie intermédiaire (52) entre ladite tige et ladite tête, ladite deuxième tige (51) ayant un diamètre extérieur inférieur audit deuxième diamètre de sorte que ledit deuxième élément de fixation d'engagement avec un os (50) peut être inséré à travers ledit au moins un trou (34) depuis ladite surface supérieure de ladite plaque (31), ladite deuxième tête élargie (54) définissant une surface partiellement sphérique (57) complémentaire audit renforcement sphérique (75) dudit au moins un trou (34), et ladite deuxième partie intermédiaire (52) ayant une partie avec un quatrième diamètre qui est approximativement égal audit deuxième diamètre, moyennant quoi ladite deuxième tête (54) dudit deuxième élément de fixation d'engagement avec un os (50) ne peut pas être pivotée à l'intérieur de ladite partie renforcée (75) dudit au moins un trou (34) de sorte que ledit deuxième élément de fixation d'engagement avec un os prend une orientation fixe par rapport à ladite surface inférieure (37) de ladite plaque (31) lorsque la deuxième tête élargie est insérée dans la partie renforcée; caractérisé en ce que:

- a) l'ouverture (77) présente une section circulaire et définit une paroi cylindrique dont le diamètre est égal au deuxième diamètre;
- b) la partie du deuxième élément de fixation d'engagement avec un os (50) qui possède le quatrième diamètre est cylindrique.
2. Système d'ostéosynthèse selon la revendication 1, comprenant en outre un ensemble à vis de blocage (33) pour verrouiller lesdites têtes desdits éléments de fixation d'engagement avec un os (50; 60) dans ladite partie renforcée sphérique (75) de ladite plaque (31).
3. Système d'ostéosynthèse selon la revendication 2, dans lequel ledit ensemble à vis de blocage (33) comprend:
- un alésage de fixation (70) défini dans ladite plaque (31) à proximité dudit au moins un trou (34);
- une rondelle (90) définissant une ouverture centrale (93) et un renforcement (94) communiquant avec ladite ouverture, ladite rondelle présentant en outre une surface extérieure circonferentielle (91) configurée pour contacter ladite tête (54; 64) dudit élément de fixation d'engagement avec un os (50; 60) s'étendant à travers ledit au moins un trou (34); et
- un élément de fixation de blocage (85) comportant une tête (87) configurée pour être enfoncée dans ledit renforcement (94) de ladite rondelle (90) et une tige allongée s'étendant à travers ladite ouverture centrale (93) et configurée pour s'insérer dans ledit alésage de fixation (70) de ladite plaque (31).
4. Système d'ostéosynthèse selon la revendication 3, dans lequel ladite surface extérieure circonferentielle (91) de ladite rondelle (90) présente une courbure concave correspondant sensiblement à ladite surface partiellement sphérique (57; 67) de ladite tête dudit élément de fixation d'engagement avec un os (50; 60).
5. Système d'ostéosynthèse selon la revendication 3 ou 4, dans lequel ladite plaque (31) définit en outre un renforcement de blocage (71) dans ladite surface supérieure concentrique avec ledit alésage de fixation (70) et ledit au moins un trou (34) comprend un renforcement évasé (79) chevauchant ledit renforcement de blocage (71).
6. Système d'ostéosynthèse selon les revendications 3, 4 ou 5, dans lequel la rondelle (90; 120) présente une surface inférieure configurée pour contacter ladite tête dudit élément de fixation d'engagement avec un os lorsque ledit élément de fixation d'engagement avec un os s'étend à travers ledit au moins un trou, ladite rondelle (120) définissant en outre une surface circonferentielle comportant une première partie (127) chevauchant ledit au moins un trou (34) lorsque ladite rondelle est dans une première position par rapport audit au moins un trou, et comportant une deuxième partie (128) qui ne chevauche pas ledit au moins un trou lorsque ladite rondelle est tournée de ladite première position vers une deuxième position, moyennant quoi ledit élément de fixation d'engagement avec un os peut être inséré à travers ledit au moins un trou, ladite rondelle étant insérée dans ladite plaque lorsque ladite rondelle est dans ladite deuxième position.
7. Système d'ostéosynthèse selon l'une quelconque des revendications 3, 4, 5 ou 6, comprenant en outre une encoche (110) définie dans ladite plaque (31) à proximité dudit alésage de fixation, ladite rondelle comprenant une clavette (129) à proximité de ladite ouverture centrale configurée pour se loger dans ladite encoche dans ladite plaque afin d'empêcher la rotation de ladite rondelle par rapport à ladite plaque.
8. Système d'ostéosynthèse selon l'une quelconque des revendications précédentes, dans lequel la plaque allongée définit une pluralité de noeuds vertébraux (35) sur la longueur de la plaque.
9. Système d'ostéosynthèse selon la revendication 8, dans lequel au moins deux trous (34) sont disposés au niveau d'un noeud (35) correspondant.
10. Système d'ostéosynthèse selon l'une quelconque des revendications précédentes, dans lequel ladite plaque allongée (31) présente un bord arrondi (36) s'étendant entre lesdites surfaces supérieure et inférieure.
11. Système d'ostéosynthèse selon l'une quelconque des revendications précédentes, dans lequel les têtes d'éléments de fixation comprennent une surface supérieure tronquée (56).
12. Système d'ostéosynthèse selon l'une quelconque des revendications précédentes, dans lequel les filetages d'engagement avec un os desdits premiers et deuxièmes éléments de fixation d'engagement avec un os (50; 60) sont auto-taraudeurs.
13. Système d'ostéosynthèse selon l'une quelconque des revendications précédentes, dans lequel ledit troisième diamètre est d'environ 2,90 millimètres et ledit quatrième diamètre est d'environ 4,05 millimètres.

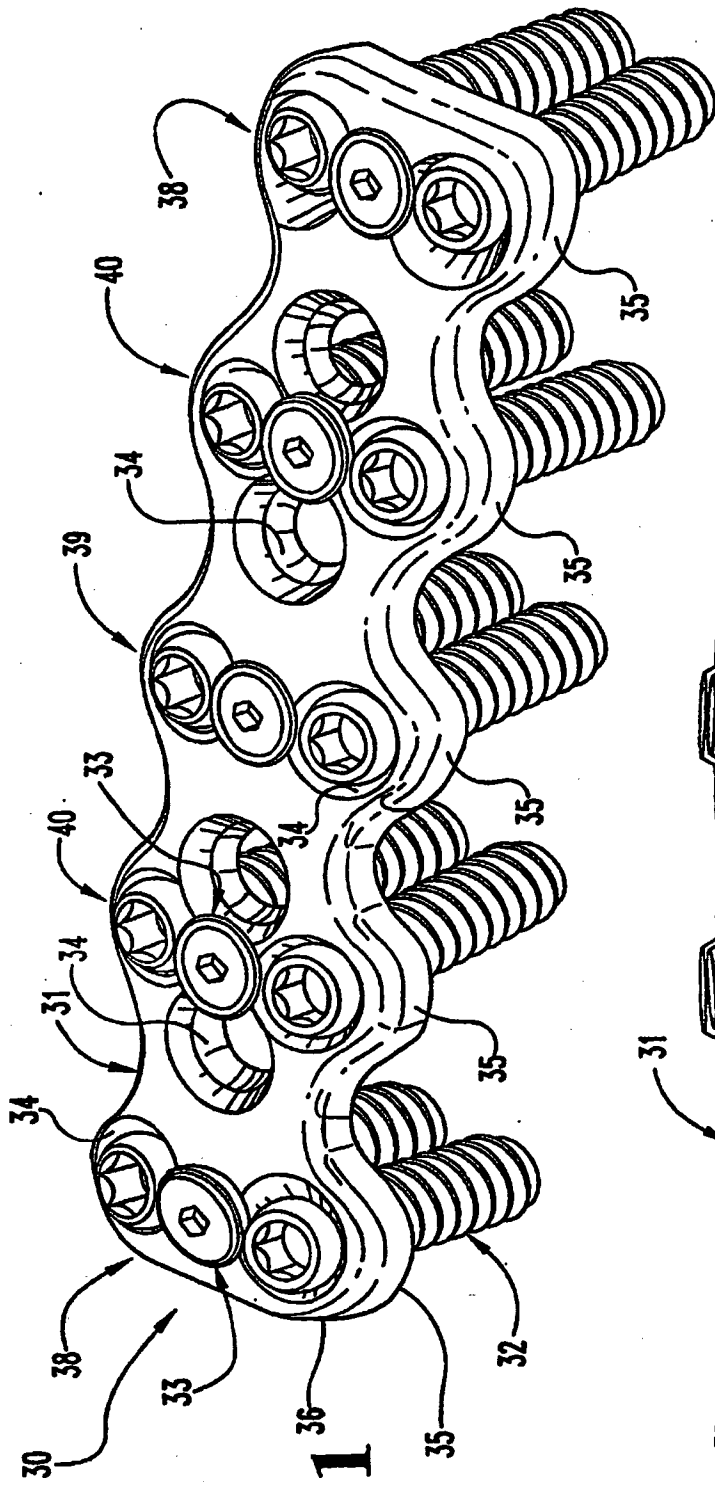


Fig. 1

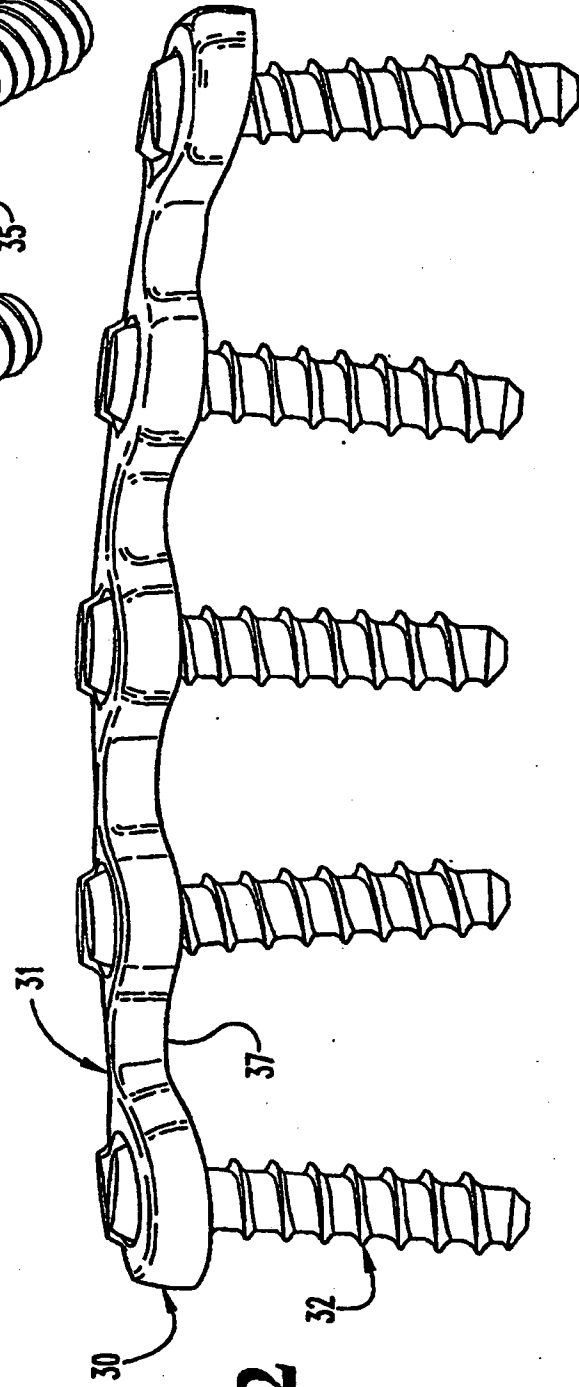


Fig. 2

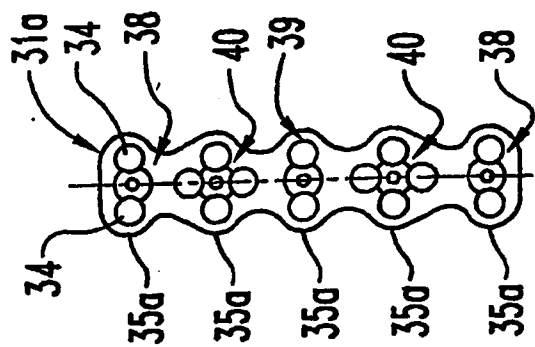


Fig. 3a

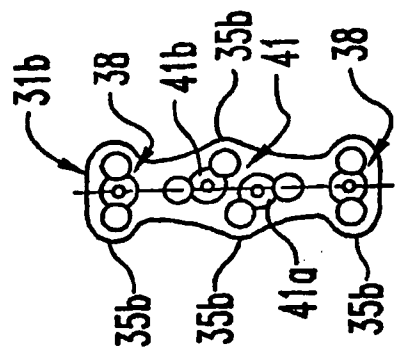


Fig. 3b

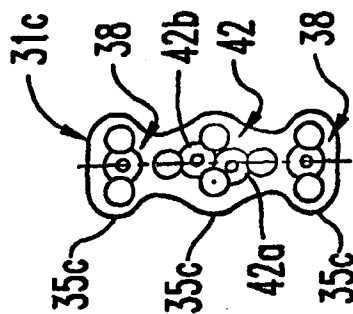


Fig. 3c

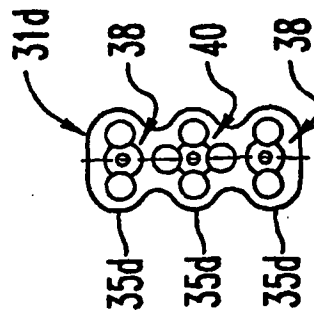


Fig. 3d

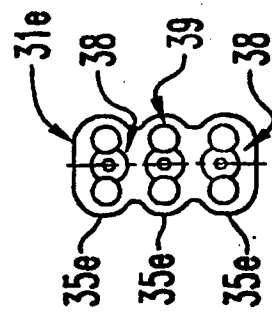


Fig. 3e

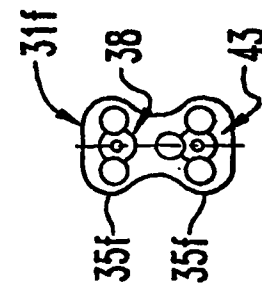


Fig. 3f

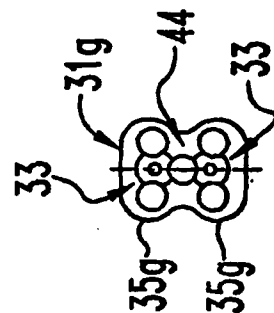


Fig. 3g

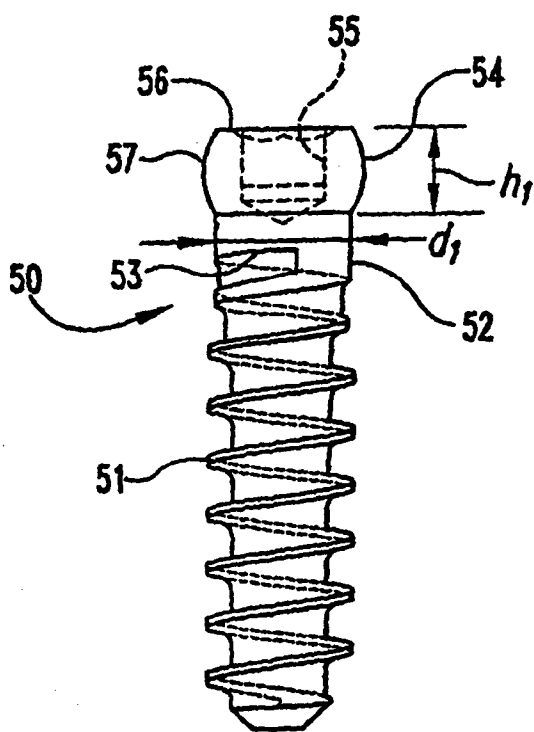


Fig. 4

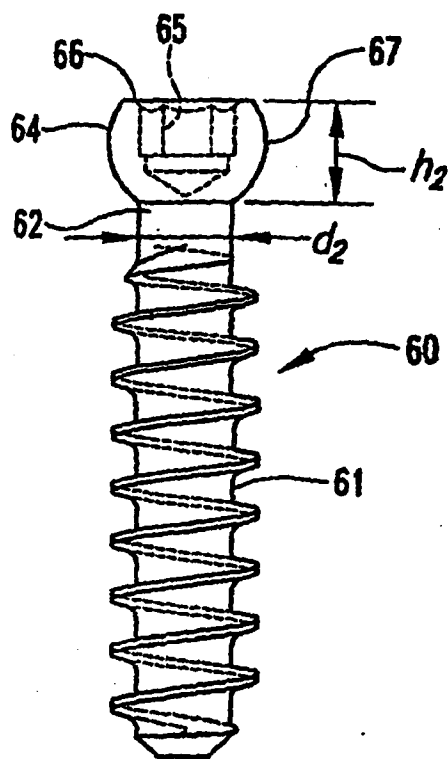


Fig. 5

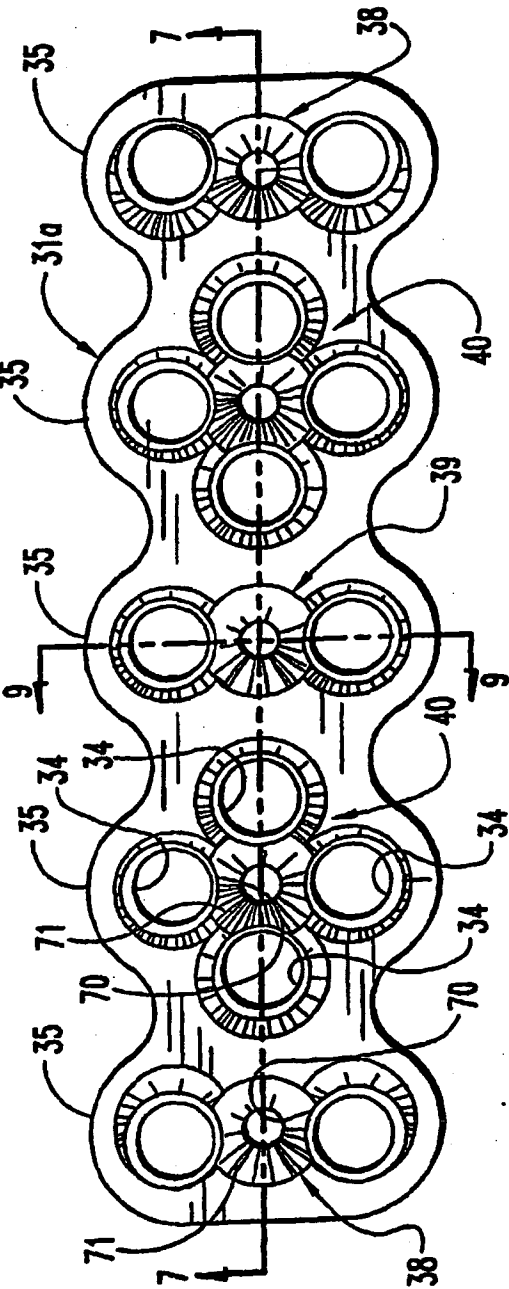


Fig. 6

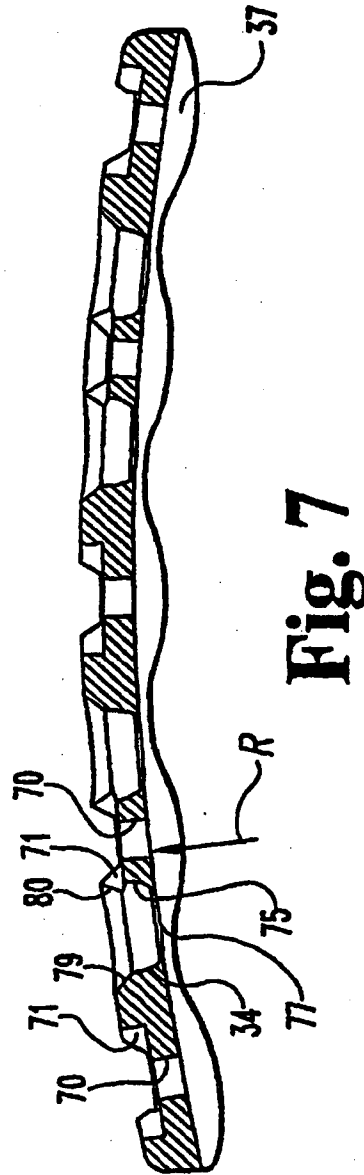


Fig. 7

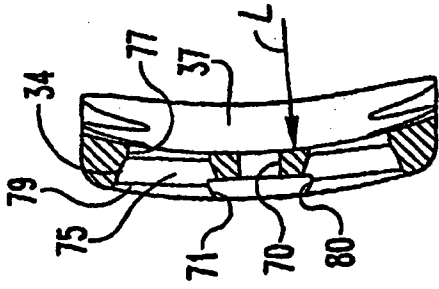


Fig. 9

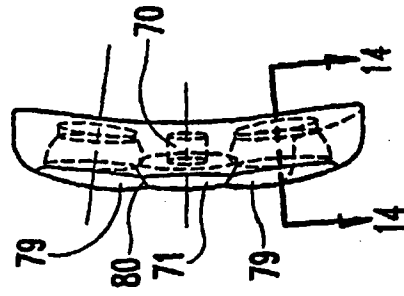


Fig. 8

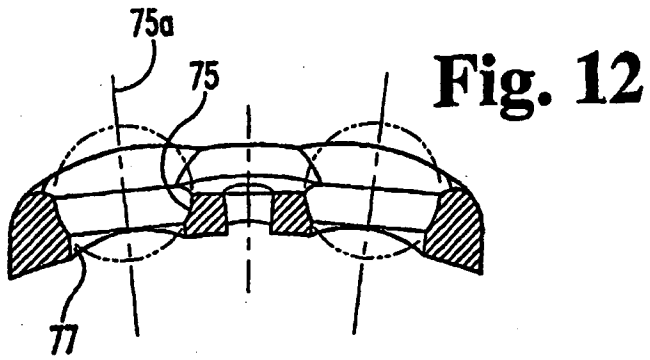


Fig. 12

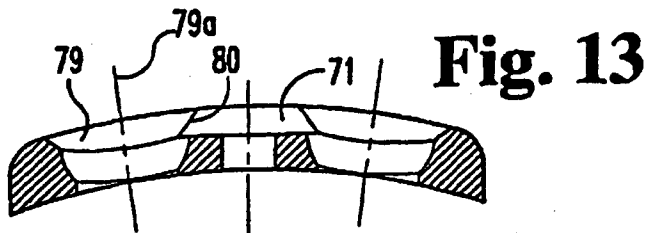


Fig. 13

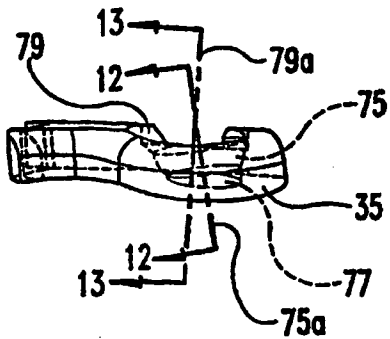


Fig. 11

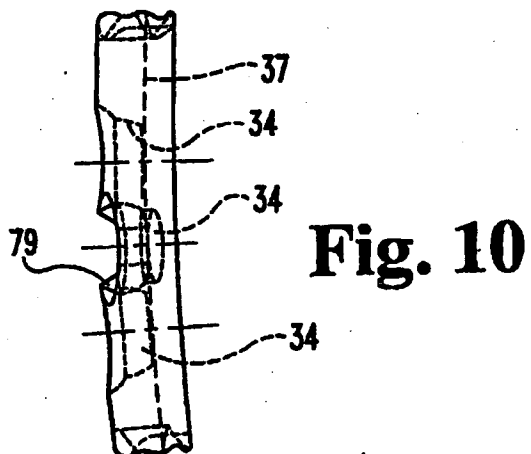


Fig. 10

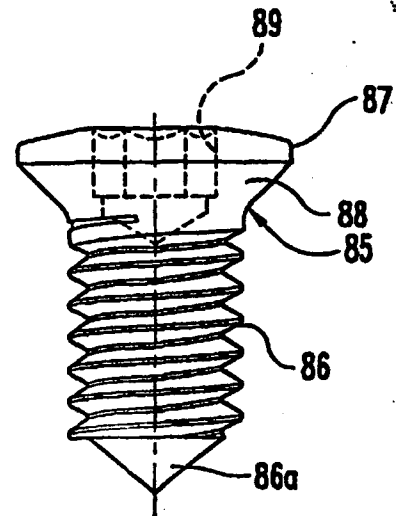


Fig. 15

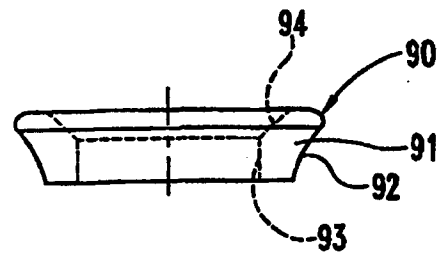


Fig. 16

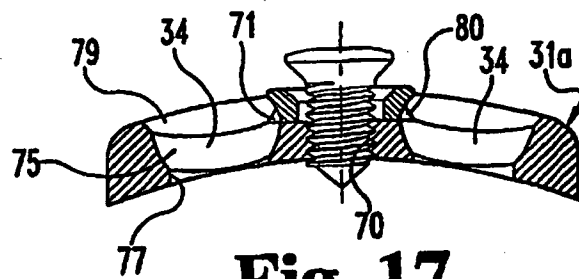


Fig. 17

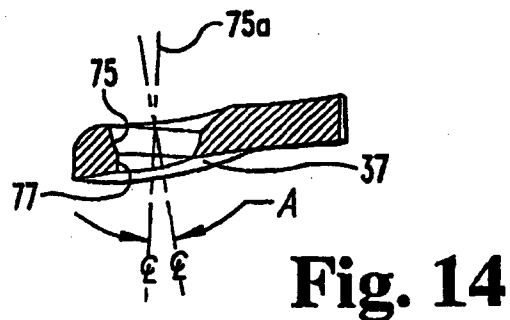


Fig. 14

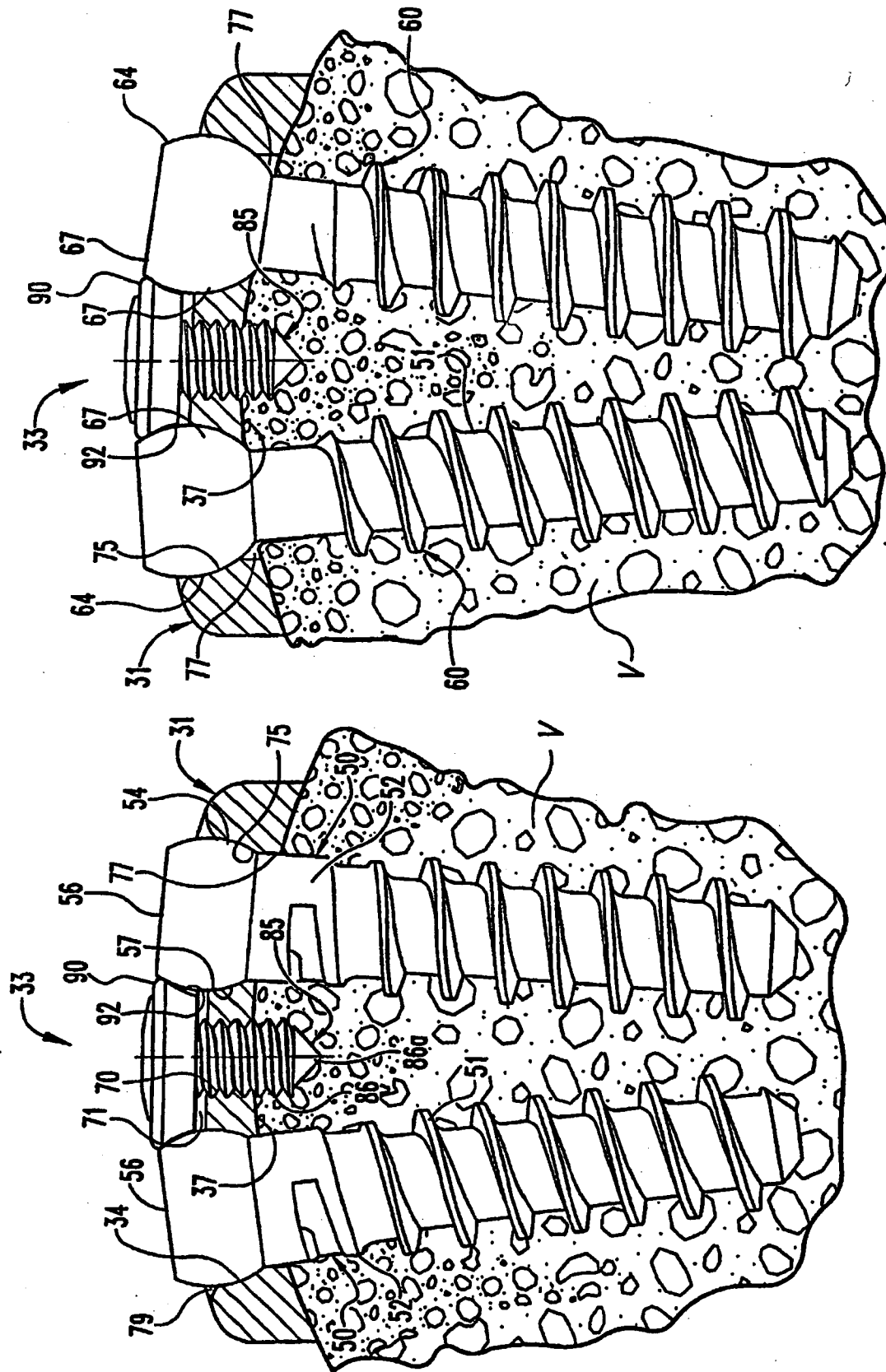


Fig. 18

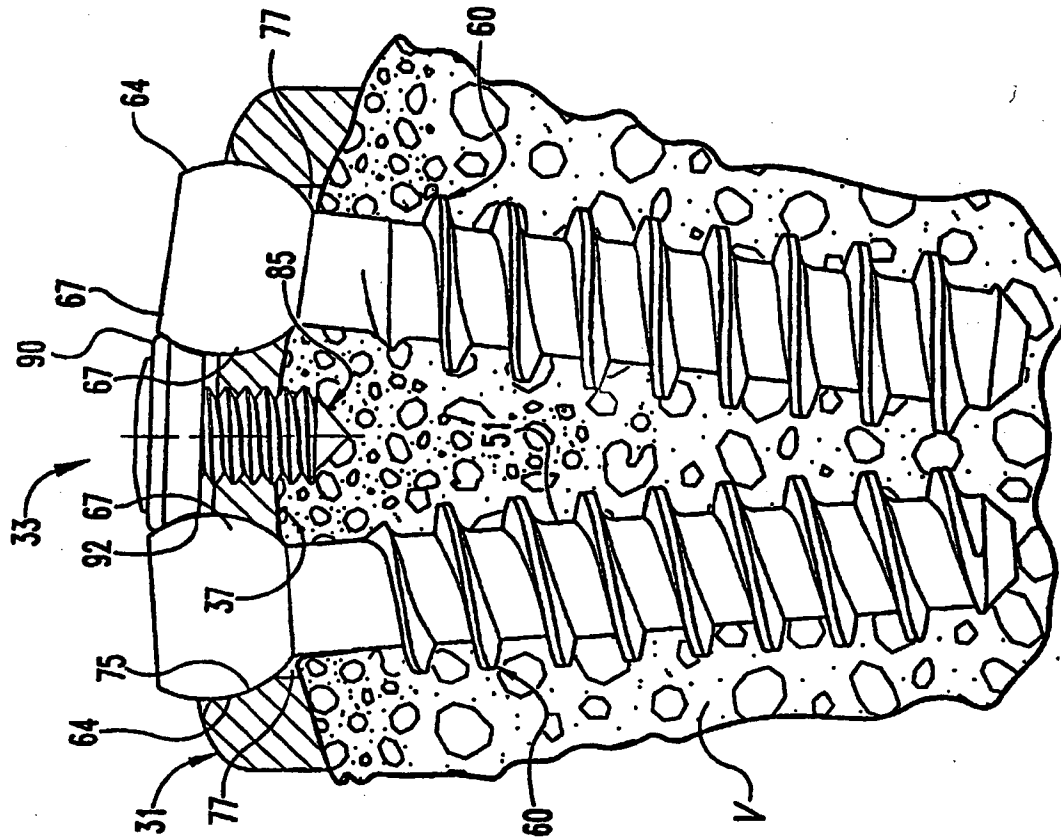


Fig. 19

Fig. 20

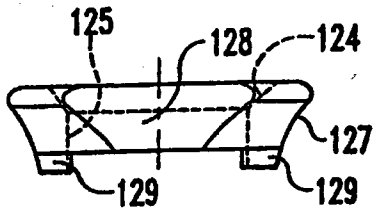
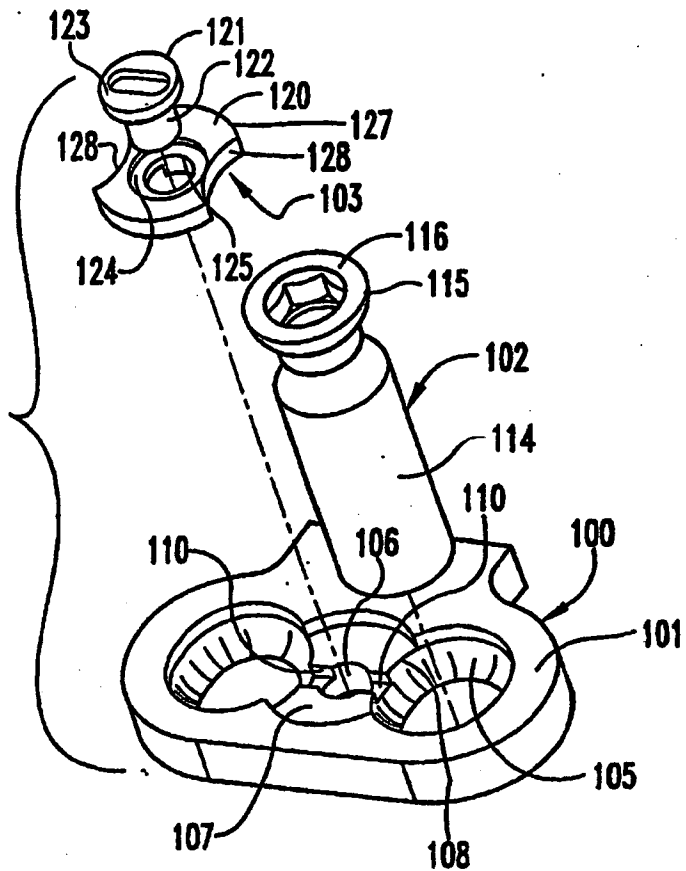


Fig. 23

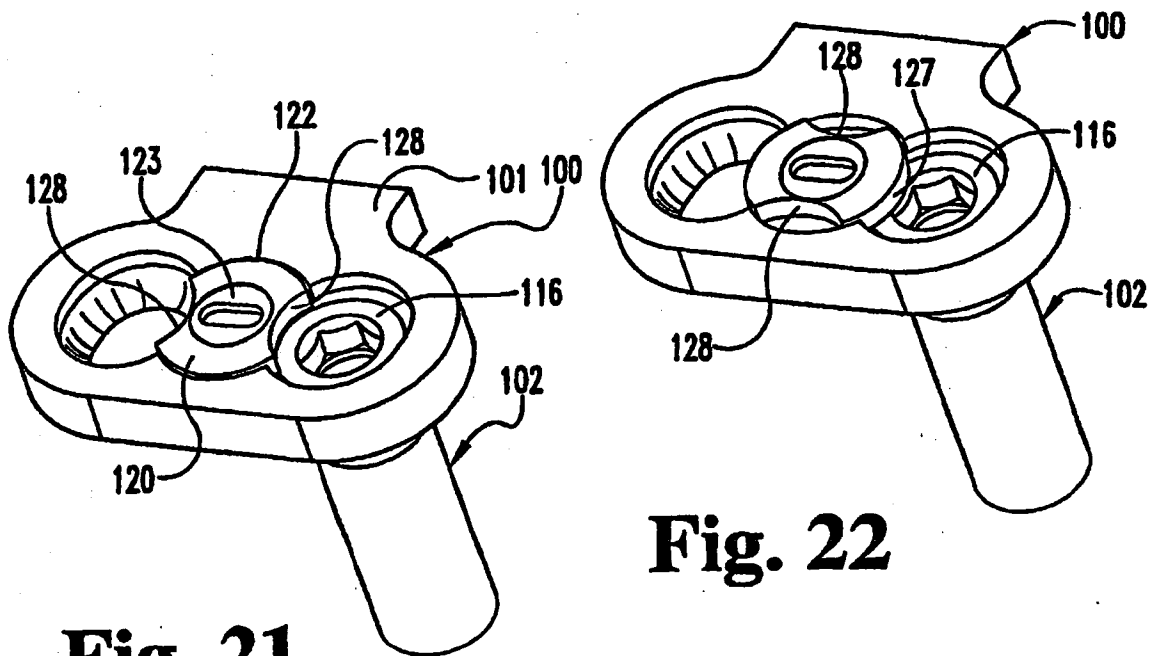


Fig. 21

Fig. 22